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(12) INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

(19) World Intellectual Property Organization  
International Bureau



(43) International Publication Date  
28 June 2001 (28.06.2001)

PCT

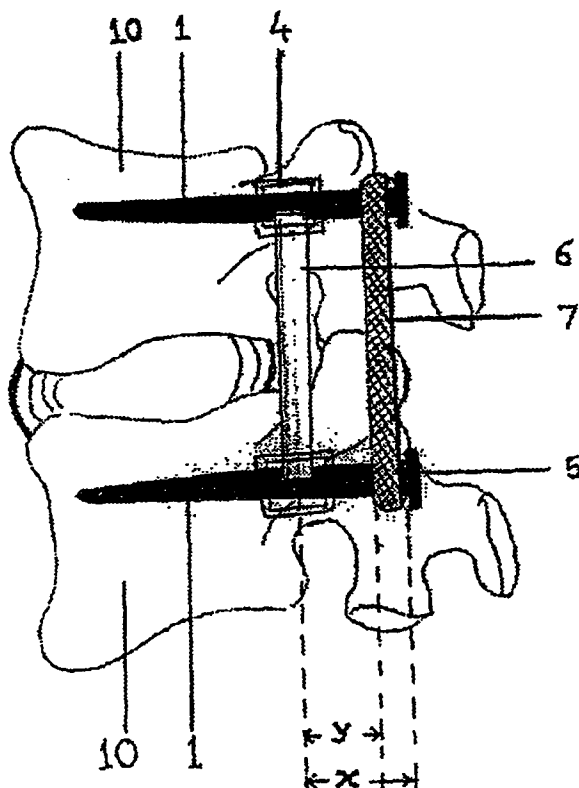
(10) International Publication Number  
**WO 01/45576 A1**

- (51) International Patent Classification<sup>7</sup>: **A61B 17/70**
- (21) International Application Number: **PCT/CH99/00612**
- (22) International Filing Date:  
20 December 1999 (20.12.1999)
- (25) Filing Language: **English**
- (26) Publication Language: **English**
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- (81) Designated States (national): **AU, BR, CA, JP, MX, NZ, US, ZA.**
- (84) Designated States (regional): **European patent (AT, BE, CH, CY, DE, DK, ES, FI, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE).**
- Published:  
— *With international search report.*

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*For two-letter codes and other abbreviations, refer to the "Guidance Notes on Codes and Abbreviations" appearing at the beginning of each regular issue of the PCT Gazette.*

(54) Title: **DEVICE FOR THE STABILISATION OF TWO ADJACENT VERTEBRAL BODIES OF THE SPINE**



(57) Abstract: The assembly is used for the stabilisation of two adjacent vertebral bodies (10) of the spine. It comprises two pedicle screws (1), having a threaded shaft (2) with a tapering first end (3) for introduction into the vertebral bodies (10) and a head portion (4) with a second end (5). It further comprises a flexible longitudinal fulcrum (6) with two portions (8), which can be disposed transversely to said pedicle screws (1), and fixed with its end portions (8) to the head portions (4) of said two pedicle screws (1) at a distance  $x$  from said second end. The assembly further comprises an elastic ligament (7) which can be disposed transversely to said two pedicle screws (1) and fixed to the head portions (4) of said two pedicle screws (1) at a distance  $y < x$  from the end portion of the fulcrum (8). By introduction of a fulcrum, lying close to the axis of flexion and extension of the spinal motion segment, the posteriorly placed ligament distracts the whole disc, and the fulcrum itself becomes a load-bearing structure. This reduces the load over the disc, and makes it an even distribution of load across the end-plate throughout the range of movement of the motion segment, that is allowed by the implant.

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**Device for the stabilisation of two adjacent vertebral bodies of the spine**

This invention concerns a device in accordance with the pre-characterising portion of Claim 1.

The human spine consists of blocks of bony vertebra with intervening blocks of soft-tissue, the intervertebral discs. These functional elements allow the spine to be flexible, and to transfer load evenly over the lower vertebra, despite variation in the position of the upper vertebra. They function as a fluid filled bag between each vertebra. However, with disc degeneration, they become anisotropic and transmit load irregularly over the endplate and this irregular loading pattern in different positions of the spine is associated with back pain.

Conventional treatment of this disorder is to fuse the two vertebrae together. This method of treatment is not attended by a high level of success. This is in part related to the stiff segment created by the fusion operation, which produces problems to the adjacent spinal segments above and below. The ideal solution would be one that allows normal load transmission and also allows movement as achieved with artificial joints elsewhere in the human body. However, the artificial disc prostheses, which have been proposed so far, have not to date produced any better results than fusion. This is in part because insertion of an artificial disc involves major surgery, and there is the difficulty in accurately placing the device to ensure that the segmental movement of the facet joints remains normal.

There are two further devices described in the treatemnt of low back pain, known as "soft-stabilisation" in which pedicle screws are placed in the vertebrae, and a stretchable ligament is attached behind, at their head portions. In both the devices, the restraining

ligaments are well behind the axis of flexion/extension. In one of these systems (Dyesys-Sulzer), whilst excessive lordosis is prevented by a cylinder embracing the ligament, the actual distraction of the posterior disc space can only be achieved by producing flexion of the segment. It is known that a kyphotic segment in the lumbar spine can produce back pain.

In the other of these systems (Graf ligament), distraction of the anterior disc space and creation of physiological lordosis is accompanied by compression of the posterior part of the disc. This results in narrowing of the diameter of the exit foramen of the nerve root, and also increases load transfer to the posterior part of the disc. It is known that increased load transfer by the posterior annulus can produce annular tear. Neither system addresses therefore the important aims of producing uniform disc distraction and the creating a normal loading pattern across the end-plate of the vertebrae.

The invention as claimed, aims at solving the problems described above.

The present invention provides a device as defined in Claim 1. By introduction of a fulcrum, lying close to the axis of flexion and extension of the spinal motion segment, the posteriorly placed ligament distracts the whole disc, and the fulcrum itself becomes a load-bearing structure. This reduces the load over the disc, and makes it an even distribution of load across the end-plate throughout the range of movement of the motion segment, that is allowed by the implant.

Clinically the ligament is applied to the assembly under tension and the fulcrum under compression at the resting position of the spine. The screws are introduced posteriorly through the pedicles on either side, so that there is an assembly of screws, fulcrums and ligaments on right and left side in the posterior aspect of the vertebrae to be stabilised. the same system can also be extended over more than one motion segment, if necessary.

The fulcrum lies closer to the axis of movement of flexion-extension of the lumbar spine. When the assembly is introduced into the spine, it allows movement of the spine in

flexion-extension, as well as in other directions. During flexion-extension, the range of movement of the fulcrum is less than that of the ligament, since the former lies closer to the axis of the movement.

The ligament actually elongates during flexion and recoils during extension. During flexion, the fulcrum bends, and also to some extent, compresses itself. These movements are reversed in extension. The two ends of the fulcrum, being tightly fixed to the pedicle screws, prevent any movement between the pedicle screws and the fulcrum at their junction.

The pedicle screws will preferably be made up of titanium and with diameters of 5, 6, 7, and 8 mm. The pedicle screw has a head portion and a threaded shaft portion. The length of the threaded shaft portion of the screw is preferably between 35 and 55 mm, with 5 mm increments. The length of the head portion is preferably of different sizes, e.g. 20, 30 and 40mm.

The distance x is preferably in the range of 10 – 20 mm and the distance y is preferably in the range of 7 to 17 mm (Fig. 1).

The fulcrum should (at least partially) be compressible in the longitudinal direction. In a preferred embodiment the fulcrum consists of a longitudinal main body of which at least its middle portion consists of a flexible material and two end portions consisting of a rigid material (e.g. the same as that of the pedicle screws). The two end portions can be designed as a sleeve over the main body.

The main body of said fulcrum is preferably made of a flexible polymer, e.g. a high-density polyethylene (HDP) with a modulus of elasticity between 17'000 to 28'000 kg/cm<sup>2</sup> or a poly tetra-fluoro ethylene (PTFE) with modulus of elasticity between 3000 to 6500 kg/cm<sup>2</sup>. The outer diameter at the metallic ends of the fulcrum is preferably between 5, 6, or 7 mm. The flexibility of the fulcrum will depend on the design and the diameter as well.

The fulcrum is preferably covered with a fabric sleeve. This has the advantage that it can resist the wear resulting from friction of the relatively soft material of the fulcrum against the bone and the soft tissues around, in the spine.

Preferably the fulcrum is drum-shaped in order to prevent buckling during bending.

Preferably the head portions of the pedicle screws are provided with a fixation mechanism for accommodating and fixing an end portion of the fulcrum.

The head portion of the pedicle screw is provided with a smooth seat for receiving the ligament, a groove for receiving the end portion of the fulcrum, and a threaded portion for receiving a locking nut.

In a preferred embodiment the assembly has a fastening mechanism to tighten the end portion of the fulcrum to the head of the pedicle screws. The fastening mechanism preferably comprises of a sleeve which can be passed over the end portion of the fulcrum, after the latter is seated into the groove in the head portion of the pedicle screw.

In a further preferred embodiment the assembly comprises of a locking nut which can be tightened over the corresponding threaded part in the head of the pedicle screw, fastening the sleeve and the end portion of the fulcrum to the head of the pedicle screw.

In a further preferred embodiment the ligament has the shape of a closed loop, which can be passed over the second end of the pedicle screw, to sit on the smooth part of the head portion of the pedicle screw. It may further comprise a cap nut which can be screwed into the second end of the pedicle screw to retain the ligament in place.

The ligament is preferably made up with braided polyester. The diameter of the cross section of the ligament can vary between 3 and 7 mm. The breaking strength should be between 2000 N and 5000 N load, depending on the diameter of the ligament, and rate of loading. The strain will be between 10 and 30 % under physiological loading.

**In the drawings:**

- Fig. 1            Shows a schematic representation of a longitudinal section through the assembly according to the invention;
- Fig. 2a           shows a side view of the fulcrum, attached to a pedicle screw in the assembly according to the invention;
- Fig. 2b           shows the pedicle screw, the fastening mechanism of the fulcrum to it, and the cap nut, before they are assembled together;
- Fig. 2c           shows the profile of the pedicle screw and the sleeve of the fastening mechanism;
- Fig. 3            shows the assembly of the pedicle screw, the fulcrum, and the ligament together for one side of the spinal segment; and
- Fig. 4            shows the assembly applied to one spinal motion segment, shown in a plastic model of the lumbar spine, from a posterior oblique view.

The assembly as shown in Fig. 1 is used for the stabilisation of two adjacent vertebral bodies 10 of the spine. It comprises two pedicle screws 1, having a threaded shaft 2 with a tapering first end 3 for introduction into the vertebral bodies 10 and a head portion 4 with a second end 5 which are shown in more detail in Figs. 2b and 2c.

The pedicle screw is made up of titanium and its diameter is 7 mm (which may vary between 5 and 8 mm). The length of the threaded portion of the pedicle screw is 45 mm (which may vary between 35 and 55 mm, with 5 mm increments). The length of the head portion up to its said second end is 30 mm (which may vary between 20 and 40 mm).

As shown in Fig. 2a, a flexible longitudinal fulcrum 6 with two end portions 8, can be disposed transversely to the pedicle screws 1, and fixed with its end portions 8 to the head portion 4 of the two pedicle screws 1, at a distance of 15 mm (which may vary between 10 and 20 mm) from the said second end 5 as shown in Fig. 1. The main body 9 of the fulcrum 6 consists of a flexible material, similar to 'high density polyethylene' (HDP) with a modulus of elasticity of  $22'500 \text{ kg/cm}^2$  (which may vary between  $17'000$  and  $28'000 \text{ kg/cm}^2$ ) or 'poly tetra-fluoro ethylene (PTFE) with a modulus of elasticity of  $4'750 \text{ kg/cm}^2$  (which may vary between  $3'000$  and  $4'500 \text{ kg/cm}^2$ ). The two end portions 8 consist of a metallic sleeve, between 15 and 20 mm long, over the flexible material of the fulcrum. The outer diameter of these metallic end portions 8 are 6 mm (which may vary between 5 and 8 mm). The fulcrum 6 is drum shaped, with larger diameter in its middle compared to the ends. The fulcrum is at least partially compressible in the longitudinal direction.

As shown in Figs. 3 and 4, the ligament 7 has the shape of a loop, which can be passed over the second end 5 of the pedicle screw, to sit on the smooth part 12 of the head portion 4 of the pedicle screw. The diameter of the cross section of the ligament is 5 mm (which may vary between 3 and 7 mm) and its breaking strength is  $3'500 \text{ N}$  load in tension (which may vary between  $2'000$  and  $4'500 \text{ N}$ ). The strain of the ligament is 20 % under physiological loading.

The elastic ligament 7 made up of braided polyester. The ligament 7 is disposed transversely to the said pedicle screws 1, and fixed to the head portions 4 of the pedicle screws 1 at a distance of 12 mm (which may vary between 7 and 17 mm) from the groove 14 for the fulcrum in the head of the pedicle screw.

Alternatively the ligament may consist of a single length flexible cord, which is made up with an outer layer of braided polyester, and an inner core of stretchable material like Dyneema (which is registered trademark of DSM High Performance Fibres B.V., Netherlands) or similar. The single length version (as opposed to the above described

loop version) of the ligament has metal sleeves at its ends for fastening it to the second end (5) of the pedicle screws.

As shown in Fig. 2c the head portions 4 of the pedicle screws 1 are provided with a fixation mechanism 12,14,16 for accommodating and fixing an end portion 8 of the fulcrum 6. The head portion 4 of the pedicle screw 1 is provided with a smooth seat 12 at its free end for receiving the ligament 7 (Fig. 1), a groove 14 for receiving an end portion 8 of the fulcrum 6, and a threaded portion 16 located between the groove 14 and the smooth seat 12 for receiving a locking nut 11.

As shown in Fig. 2c the head portion 4 of the pedicle screws 1 consists of three segments 12,14,16 for accommodation and fixation of the end portions 8 of the fulcrum 6. These are, a smooth seat 12 at its free end for receiving the ligament 7, a groove 14 for receiving the end portion 8 of the fulcrum 6, and a threaded portion 16, located between the smooth seat and the groove, for receiving the locking nut 11.

As shown in Fig. 2a the end portion 8 of the fulcrum 6 is fastened to the head portion 4 of the pedicle screw with a sleeve 17 and a nut 11. The fastening mechanism 13 is shown in more detail in Fig. 2b. It comprises a sleeve 17 which can be passed over the end portions 8 of the fulcrum 6 after the latter is seated into the groove 14 in the head portion 4 of the pedicle screw. It further comprises a locking nut 11, which can be tightened over the corresponding threaded portion 16 in the head portion 4 of the pedicle screw, fastening the sleeve 17 and the end portion 8 of the fulcrum, to the pedicle screw. Finally a cap nut 15 can be screwed into the second end 5 of the pedicle screw, to retain the ligament in place.

In Fig. 3 the completed assembly is represented with the fulcrum 6 fixed to the two pedicle screws 1 and the ligament 7 wound and secured on the head portions 4 of the pedicle screws 1.



In Fig. 4 two pairs of assemblies are shown implanted in the spine model. On the right hand assembly only the fulcrum 6 has been fixed to the head portion 4 of the pedicle screws 1, whereas on the left hand assembly (having a different type of fulcrum) the ligament 7 has also been applied thereto.

### Claims

1. Assembly for the stabilisation of two adjacent vertebral bodies (10) of the spine comprising of two pedicle screws (1), having a threaded shaft (2) with a tapering first end (3) for introduction into the vertebral bodies (10) and a head portion (4) with a second end (5), characterized by
  - (A) a flexible longitudinal fulcrum (6) with two portions (8), which can be disposed transversely to said pedicle screws (1), and fixed with its end portions (8) to the head portions (4) of said two pedicle screws (1) at a distance  $x$  from said second end; and
  - (B) an elastic ligament (7) which can be disposed transversely to said two pedicle screws (1) and fixed to the head portions (4) of said two pedicle screws (1) at a distance  $y < x$  from the end portion of the fulcrum (8).
2. Assembly according to claim 1, characterized in that said fulcrum (6) is at least partially compressible in the longitudinal direction.
3. Assembly according to claim 1 or 2, characterized in that said distance  $x$  is in the range of 10 – 20 mm.
4. Assembly according to one of the claims 1 to 3, characterized in that said distance  $y$  is in the range of 7 to 17 mm.
5. Assembly according to one of the claims 1 to 4, characterized in that said fulcrum (6) comprises
  - A) a longitudinal main body (9) of which at least its middle portion consists of a flexible material ; and
  - B) two end portions (8) consisting of a rigid material.

6. Assembly according to claim 5, characterized in that said two end portions (8) are designed as a sleeve over said main body (9).
7. Assembly according to claim 5, characterized in that said main body (9) of said fulcrum (6) is either a high-density polyethylene (HDP) with a modulus of elasticity between 17'000 to 28'000 kg/cm<sup>2</sup> or a poly tetra-fluoro ethylene (PTFE) with modulus of elasticity between 3000 to 6500 kg/cm<sup>2</sup>
8. Assembly according to one of the claims 1 to 7, characterized in that said fulcrum (6) is covered with a fabric sleeve.
9. Assembly according to one of the claims 1 to 8, characterized in that said fulcrum (6) is drum-shaped.
10. Assembly according to one of the claims 1 to 9, characterized in that said head portions (4) of said pedicle screws (1) are provided with a fixation mechanism (12,14,16) for accommodating and fixing an end portion (8) of the fulcrum(6).
11. Assembly according to one of the claims 1 to 10, characterized in that said head portion (4) of said pedicle screw (1) is provided with a smooth seat (12) for receiving said ligament (7), a groove (14) for receiving said end portion (8) of the fulcrum (6), and a threaded portion (16) for receiving a locking nut (11).
12. Assembly according to one of the claims 1 to 11, characterized in that said head (4) is provided with a fastening mechanism (13) for tightening said end portion (8) of the fulcrum (6).
13. Assembly according to one of the claims 11 or 12, characterized in that said fastening mechanism (13) comprises a sleeve (17) which can be passed over the end portion (8) of the fulcrum (6), after the latter is seated into said groove (14) in the head portion (4) of said pedicle screw (1).

14. Assembly according to claim 13, characterized in that it comprises a locking nut (11) which can be tightened over the corresponding threaded part (16) in the head (4) of the pedicle screw (1), fastening the sleeve (17) and the head end (8) and the fulcrum to the pedicle screw(1).

15. Assembly according to one of the claims 1 to 14, characterized in that said ligament (7) has the shape of a closed loop, which can be passed over the second end (5) of the pedicle screw, to sit on the smooth part (12) of the head portion (4) of the pedicle screw.

16. Assembly according to one of the claims 1 to 15, characterized in that said ligament (7) is made up with braided polyester.

17. Assembly according to one of the claims 1 to 16, characterized in that it comprises a cap nut (15) which can be screwed into the second end of the pedicle screw (1) to retain the ligament (7) in place.

18. Assembly according to one of the claims 1 to 17, characterized in that said ligament (7) consists of a single length flexible cord, which preferably is made up with an outer layer of braided polyester, and an inner core of stretchable material.

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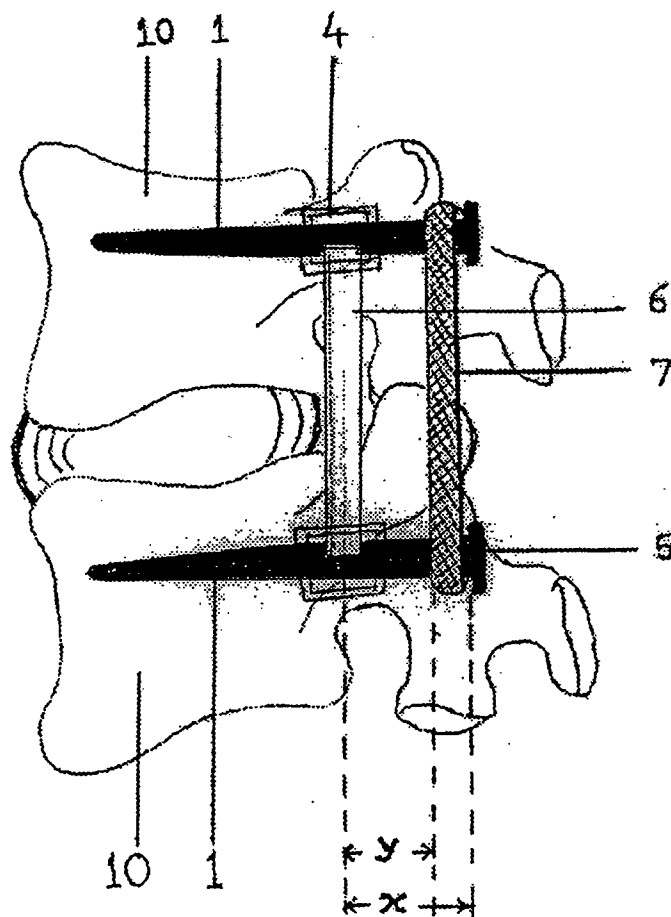


FIG. 1

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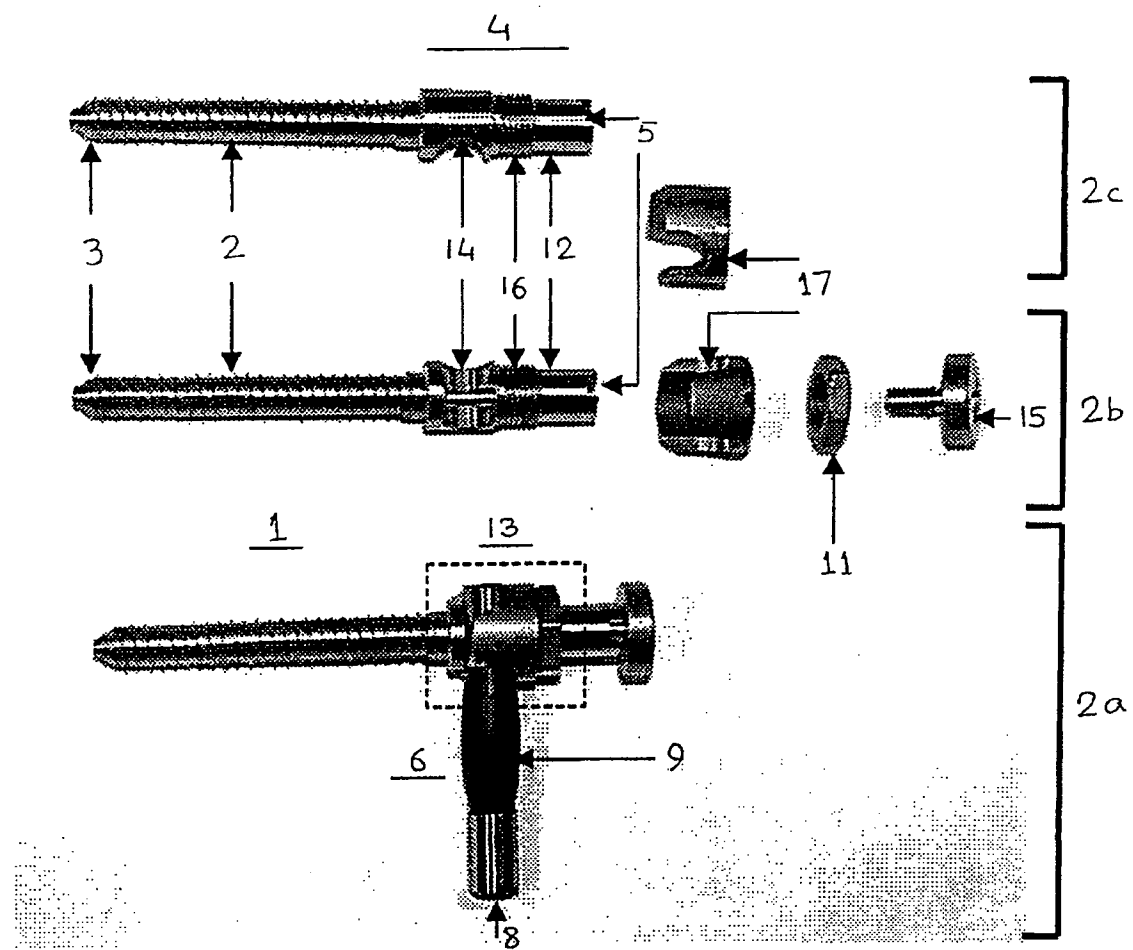


FIG 2 a, b, c

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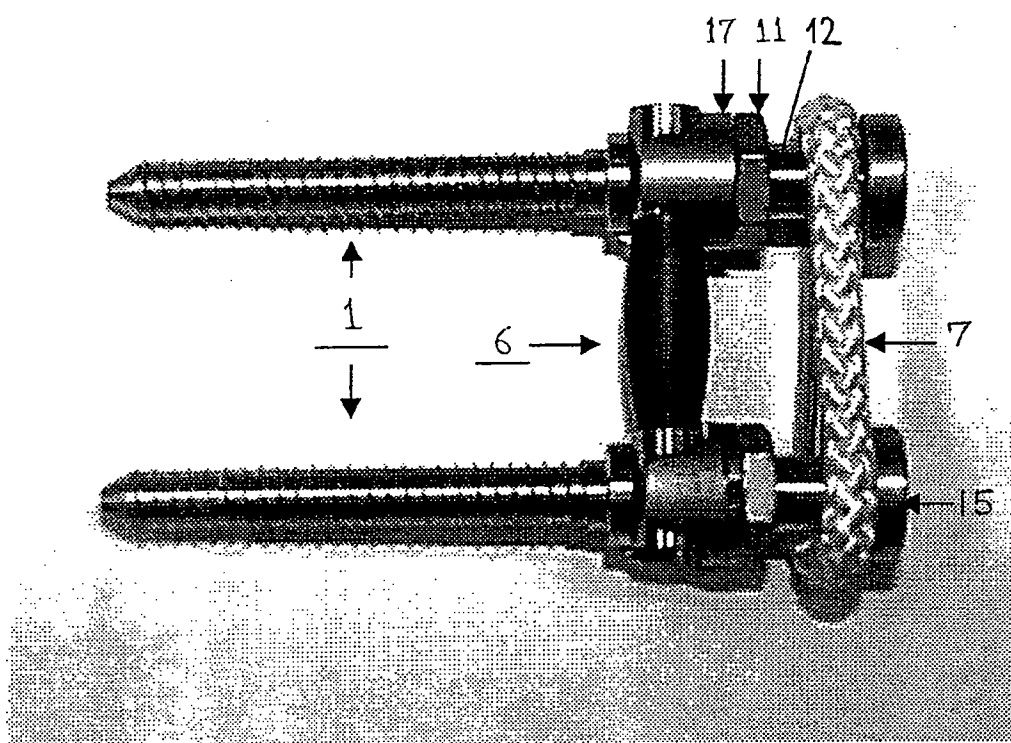


FIG. 3

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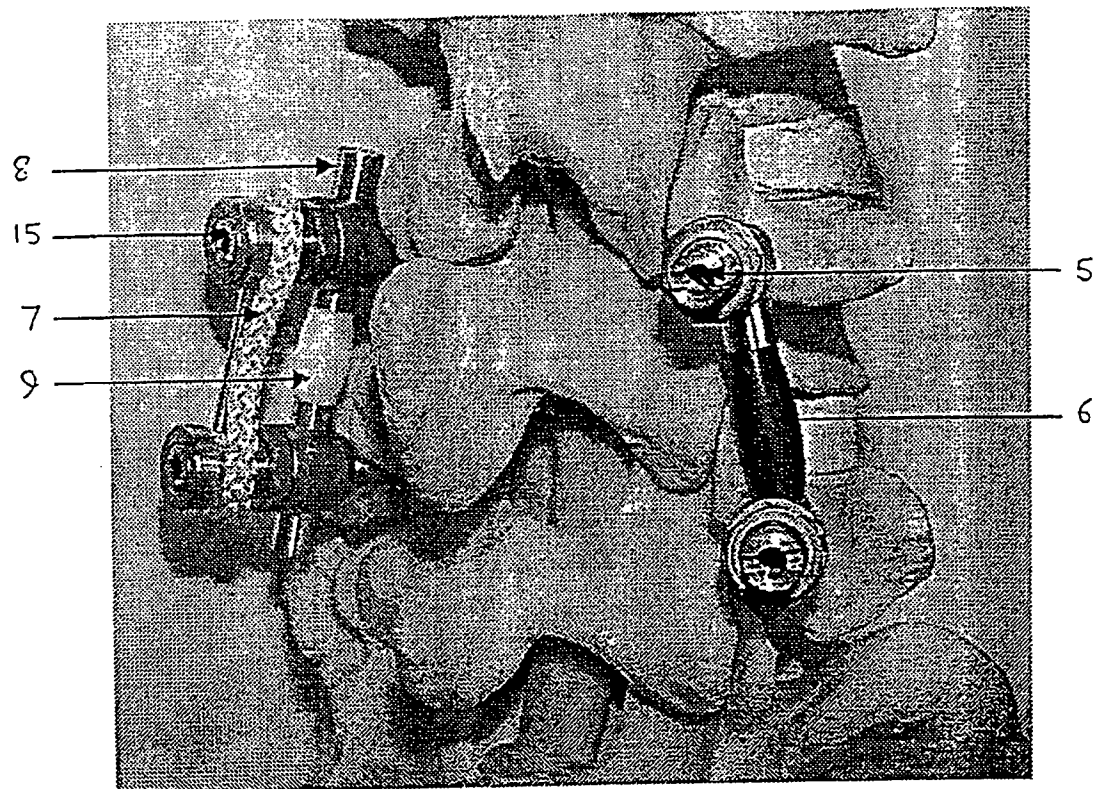


FIG. 4



## INTERNATIONAL SEARCH REPORT

International Application No

PCT/CH 99/00612

**A. CLASSIFICATION OF SUBJECT MATTER**  
IPC 7 A61B17/70

According to International Patent Classification (IPC) or to both national classification and IPC

**B. FIELDS SEARCHED**

Minimum documentation searched (classification system followed by classification symbols)

IPC 7 A61B

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practical, search terms used)

EPO-Internal

**C. DOCUMENTS CONSIDERED TO BE RELEVANT**

| Category * | Citation of document, with indication, where appropriate, of the relevant passages                                  | Relevant to claim No. |
|------------|---|-----------------------|
| A          | DE 91 12 466 U (HOWMEDICA)<br>5 December 1991 (1991-12-05)<br>the whole document                                    | 1                     |
| A          | DE 38 07 335 A (ORTHOPLANT ENDOPROTHETIK)<br>14 September 1989 (1989-09-14)<br>the whole document                   | 1                     |
| A          | EP 0 669 109 A (PROTEK AG ;SULZER<br>MEDIZINALTECHNIK AG (CH))<br>30 August 1995 (1995-08-30)<br>the whole document | 1,2,5,6,<br>9,10,12   |
| A          | FR 2 715 057 A (BREARD FRANCIS HENRI)<br>21 July 1995 (1995-07-21)<br>the whole document                            | 1                     |



Further documents are listed in the continuation of box C.



Patent family members are listed in annex.

## \* Special categories of cited documents :

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Date of the actual completion of the international search

21 August 2000

Date of mailing of the international search report

25/08/2000

Name and mailing address of the ISA

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# INTERNATIONAL SEARCH REPORT

Information on patent family members

International Application No

PCT/CH 99/00612

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